# Introducing the Differentiated All-Pole and One-Zero Gammatone Filter Responses and their Analog VLSI Log-domain Implementation

A. G. Katsiamis<sup>1</sup>, E. M. Drakakis<sup>2</sup> Department of Bioengineering (The Sir Leon Bagrit Centre) Imperial College London London, UK 1. andreas.katsiamis@imperial.ac.uk 2. e.drakakis@imperial.ac.uk

Abstract—The scope of this paper is to introduce two particular filter responses which closely resemble tuning curves at specific set of places on the basilar membrane (BM) of the biological cochlea. The responses are termed Differentiated All-Pole Gammatone Filter (DAPGF) and One-Zero Gammatone Filter (OZGF) and their form suggest their implementation by means of cascades of N identical two-pole systems, which makes them excellent candidates for efficient analog VLSI implementations. The resulting filters can be used in a filterbank architecture to realize cochlea implants or auditory processors of increased biorealism. In addition, their simple parameterization allows the use of conventional automatic gain control (AGC) schemes to model certain important features of the biological cochlea (e.g. level-dependent gain) that are observed physiologically. To illustrate the idea, we present preliminary simulation results from a 4<sup>th</sup>-order OZGF using novel high dynamic range log-domain biquads in CMOS weak inversion (CMOS-WI). All circuits were designed in Cadence® Design Framework, using the commercially available AMS 0.35µm CMOS process. The reported OZGF structure has a simulated input dynamic range of 114.5dB, while dissipating 3.7µW of static power.

## I. INTRODUCTION

The Gammatone filter (GTF), originally introduced by Johannesma in 1972 to describe cochlea nucleus response [1], is the most frequently used auditory filter in cochlea modeling [2] and speech recognition experiments [3]. The name Gammatone (or  $\Gamma$ -tone) was given by Aertsen and Johannesma after observing its impulse response which consists of a Gamma-distribution envelope times a sinusoidal tone. Its popularity, within the auditory modeling community, results from its ability to provide an appropriately shaped 'pseudo-resonant' frequency transfer function that can be used to reasonably match physiologically measured responses. However, the GTF is inherently nearly symmetric in the passband, while physiological measurements show a significant asymmetry in the biological cochlea transfer Richard F. Lyon, Fellow, IEEE Foveon Inc., 2820 San Tomas Expressway, Santa Clara CA 95051 dicklyon@acm.org

function. In addition, it is not easy to use the parameterization of the GTF to model level-dependent changes in the auditory filter.

The Gamma-distribution: 
$$At^{N-1} \exp(-bt)$$
 (1.1)

The tone:  $\cos(\omega t + \phi)$  (1.2)

The Gammatone:  $At^{N-1} \exp(-bt) \cos(\omega_{t}t + \phi)$  (1.3)

The parameters order N (integer), ringing frequency  $\omega_r$  (rad/s), starting phase  $\phi$  (rad), and one-sided pole bandwidth b (rad/s), together with (1.1) - (1.3) complete the description of the GTF.



Figure 1. The components of a Gammatone; The Gamma-distribution envelope (top), the sinusoidal tone (middle), the Gammatone impulse response (bottom).

### II. GTF, DAPGF AND OZGF TRANSFER FUNCTIONS

By expanding the cosine tone of the GTF impulse response into a sum of complex exponentials, we arrive at two terms with commonly encountered Laplace transforms:

$$g(t) = \frac{A}{2} \left\{ \exp(i\phi)t^{N-1} \exp[(-b + i\omega_{r})t] + \exp(-i\phi)t^{N-1} \exp[(-b - i\omega_{r})t] \right\}$$
(1.4)

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Using the relation  $t^{N-1} \exp(pt) \rightarrow \Gamma(N)/(s-p)^N$ , identifying p with the complex pole location  $-b + i\omega_r$  and its conjugate, we arrive at the Gammatone's Laplace transform or the GTF transfer function G(s):

$$G(s) = \frac{A\Gamma(N)}{2} \begin{cases} \exp(i\phi)[s - (-b - i\omega_r)]^N + \\ + \exp(-i\phi)[s - (-b + i\omega_r)]^N \end{cases}}{\left[(s + b)^2 + \omega_r^2\right]^N}$$
(1.5)

 $\Gamma(N)$  is the Gamma-function and is defined as  $\Gamma(N)=(N-1)!$ , whereas A can in practice be an arbitrary gain factor. Expressing b and  $\omega_r$  in terms of the pole-frequency  $\omega_o$  and quality factor Q and dropping the  $A\Gamma(N)/2$  gain term without any loss of generality, we obtain the Q-parameterization of G(s):

$$G(s) = \frac{\begin{cases} \exp(i\phi) \left[ s - \left( -\frac{\omega_o}{2Q} - i\omega_o \sqrt{1 - 1/4Q^2} \right) \right]^N + \left[ + \exp(-i\phi) \left[ s - \left( -\frac{\omega_o}{2Q} + i\omega_o \sqrt{1 - 1/4Q^2} \right) \right]^N \right]}{\left[ s^2 + \frac{\omega_o}{Q} s + \omega_o^2 \right]^N}$$
(1.6)

The above transfer function may be considered as the addition of two individual  $N^{\text{th}}$ -order complex pole terms which add with constructive or destructive interference. Note that G(s) may have a zero at s=0 for particular phases  $\phi$  of the GTF. On a dB scale this means that the low-frequency tail may head towards minus infinity at DC depending on the particular combination of  $\phi$ , N and Q. Moreover, at very high frequencies the N zeros may cancel out N of the poles resulting in an ultimate high-frequency roll-off rate of 6NdB/Oct. Fig.2 illustrates a 4<sup>th</sup>-order GTF frequency response with the phase angle  $\phi$  varying from 0 to  $\pi/2$ .



Figure 2. The GTF frequency response of order 4 and Q=1 for various phase angles.

The "spurious" zeros appearing in the numerator of the GTF transfer function are a limitation when one considers the implementation of this auditory filter in the analog domain. That probably explains why all the GTF realizations in the literature are digital implementations. Good approxima-

tions to the GTF, which keep all its important features but at the same time can be implemented efficiently in the analog domain, are the Differentiated All-Pole and One-Zero Gammatone Filters or DAPGF and OZGF respectively. The DAPGF is derived by discarding all the zeros of the GTF apart from one at DC, whereas the OZGF can have a zero anywhere on the real axis; the resulting transfer functions are described by (1.7) and (1.8):

$$H_{DAPGF}(s) = \frac{Ks}{\left[s^2 + \frac{\omega_o}{Q}s + \omega_o^2\right]^N}$$
(1.7)

$$H_{OZGF}(s) = \frac{K(s+a)}{\left[s^2 + \frac{\omega_o}{O}s + {\omega_o}^2\right]^N}$$
(1.8)

By choosing *K* to be  $\omega_o^{2N-1}$  the  $H_{DAPGF}(s)$  can be split into a product of two transfer functions, namely an All-Pole Gammatone Filter approximation (APGF) [4] (in this case, a cascade of *N*-1 identical lowpass biquads) and an appropriately scaled bandpass biquad.

$$H_{DAPGF}(s) = \frac{\omega_{o}^{2N-1}s}{[s^{2} + \frac{\omega_{o}}{Q}s + \omega_{o}^{2}]^{N}} = \frac{\omega_{o}^{2N-2}}{[s^{2} + \frac{\omega_{o}}{Q}s + \omega_{o}^{2}]^{N-1}} \times \frac{\omega_{o}s}{s^{2} + \frac{\omega_{o}}{Q}s + \omega_{o}^{2}}$$
(1.9)

Similarly, the  $H_{OZGF}(s)$  can be split into an APGF and an appropriately scaled lossy bandpass biquad (i.e. a 2-pole, 1-zero transfer function).

$$H_{OZGF}(s) = \frac{\omega_o^{2^{N-1}}(s+a)}{[s^2 + \frac{\omega_o}{Q}s + \omega_o^2]^N} = \frac{\omega_o^{2^{N-2}}}{[s^2 + \frac{\omega_o}{Q}s + \omega_o^2]^{N-1}} \times \frac{\omega_o(s+a)}{s^2 + \frac{\omega_o}{Q}s + \omega_o^2}$$
(1.10)

The beauty of the transfer functions (1.9) and (1.10), lies not only in their convenient form towards efficient analog circuit realizations, but also in their ability to exhibit realistic asymmetry in the frequency domain, providing a potentially better match to psychoacoustic data. The DAPGF exhibits a reasonable bandwidth and centre frequency variation, while maintaining a linear low-frequency tail only by varying a single level-dependent parameter (its quality factor, O). The OZGF exhibits the exact same characteristics as the DAPGF, while allowing the variation of the DC level of its low-frequency tail. To ease circuit realization, it is more practical to choose the position of the zero to change in accordance to the quality factor (in other words set  $\alpha = \omega_o/Q$ ). Lastly, it is important to note, that since the DAPGF and OZGF are essentially cascaded structures, very large gain variations can be realized while the respective quality factors are small and vary little.

How do these behaviors relate to the biological cochlea? The careful observation of Fig.3 will reveal that the actual frequency response at a particular place on the BM of the biological cochlea is an asymmetric bandpass response. The cochlea adapts itself according to the strength of the incoming input sound. For loud sounds, it becomes passive providing low (or no) gain in the passband, whereas for weak sounds it becomes highly selective with the peak gain reaching 60dB or higher. Moreover, the actual peak shifts to the right (i.e. towards higher frequencies) as the input level decreases; this shift is accompanied by an increase in spectral selectivity. This behavior is reflected in both the DAPGF and OZGF with the additional flexibility of the OZGF to adjust the DC level of its low-frequency tail.



Figure 3. Frequency domain responses obtained from the mammalian cochlea at a particular position on the BM [5]. Note that the frequency axis is in linear scale. The responses would look much more selective, if it were to be plotted in logarithmic scale.



Figure 4. The DAPGF frequency response of order 4 and with Q ranging from 1 to 10.



Figure 5. The OZGF frequency response of order 4 and with Q ranging from 1 to 10. Observe how the filter shape changes from a low peak gain lowpass shape (Q=1, loud sounds) to a pseudo-resonant bandpass like shape (Q=10, weak sounds).

We have analyzed, characterized and parameterized the DAPGF and OZGF and obtained graphs which show how gain, bandwidth, low-side dispersion and roll-off slopes can be traded-off in terms of Q and the order N. Essentially, we have provided a set of 'design curves' for fitting these responses to measured physiological data (see Fig.6 for an indicative example). These results will be published in full detail elsewhere.



Figure 6. The DAPGF Peak Gain iso-*N* responses. Observe that for a  $4^{th}$ -order DAPGF with a *Q* of 10, the overall gain is at 80dB (check with Figs.4, 5 and 11).

## III. ANALOG VLSI IMPLEMENTATION

From the preceding discussion, it can be concluded that the successful implementation of the DAPGF or OZGF lies in the ability of the engineer to create high performance biquads. By high performance, we imply high-dynamic-range and/or low-power, if the system is intended for an implantable or portable device. In this paper, we present preliminary simulation results from an OZGF designed in accordance with the architecture shown in Fig.7.



Figure 7. Simplified proposed OZGF channel architecture.

The design is comprised by eight Class-A biquads connected in a pseudo-differential Class-AB arrangement to increase the dynamic range. The biquads were implemented in CMOS-WI using the log-domain circuit technique together with a non-linear-state cross-coupling scheme to ensure that all internal currents, for the respective Class-A biquads at each branch, remain strictly positive at all times [6]. The input current conditioner was chosen to be a geometric mean splitter due to its good frequency response and lower DC levels, ensuring lower static power consumption and noise (relative to the harmonic mean splitter). Fig.8 depicts a simplified circuit schematic of the Class-AB biquad, whereas the implemented transfer functions are described by (1.11) and (1.12). Moreover, moving the positioning of the biasing current  $I_Q$  from point A to point B, results in the implementation of a 2-pole, 1-zero transfer function, described by (1.13). By inspection:  $\omega_o = I_o/nCU_T$  (where n is the subthreshold slope parameter and  $U_T$  is the thermal voltage) and  $Q = I_o/I_O$ .

$$\frac{I_{OUT_{LP}}}{I_{IN}} = \frac{W_2^U - W_2^L}{I_{IN}^U - I_{IN}^L} = \frac{(I_o/nCU_T)^2}{s^2 + \frac{(I_o/nCU_T)}{(I_o/I_Q)}s + (I_o/nCU_T)^2} (1.11)$$

$$\frac{I_{oUT_{BP}}}{I_{IN}} = \frac{W_{I}^{U} - W_{I}^{L}}{I_{IN}^{U} - I_{IN}^{L}} = \frac{(I_{o}/nCU_{T})s}{s^{2} + \frac{(I_{o}/nCU_{T})}{(I_{o}/I_{Q})}s + (I_{o}/nCU_{T})^{2}} (1.12)$$

$$\frac{I_{OUT_{2P1Z}}}{I_{IN}} = \frac{W_{1}^{U} - W_{1}^{L}}{I_{IN}^{U} - I_{IN}^{L}} = \frac{\left(\frac{I_{o}}{nCU_{T}}\right)\left[s + \frac{C_{o}/NCU_{T}}{(I_{o}/I_{Q})}\right]}{s^{2} + \frac{(I_{o}/nCU_{T})}{(I_{o}/I_{Q})}s + (I_{o}/nCU_{T})^{2}} (1.13)$$





Figure 8. Simplified circuit topology of the log-domain pseudodifferential Class-AB biquad. The feeding (by means of cascoded mirrors) of the currents  $W_i^U(W_i^L)$  to the lower (upper) topology, ensures the true Class-AB operation of the filter.

The simplified geometric mean splitter circuit is depicted in Fig.9. From the translinear loop, one can deduce that

$$I_{IN}^{\ U}I_{IN}^{\ L} = I_{BLAS}^{\ 2} \quad (1.14)$$
$$I_{IN} = I_{IN}^{\ U} - I_{IN}^{\ L} \quad (1.15)$$

In addition,

Thus,  $I_{IN}^{U}$  and  $I_{IN}^{L}$  (i.e. the inputs to the two branches of the Class-AB pseudo-differential OZGF) are kept always positive because of the geometric mean law (1.14).



Figure 9. Simplified circuit topology of the geometric mean splitter.  $I_{BLAS}$  can be set arbitrarily small to reduce the noise.

#### IV. SIMULATION RESULTS

The circuits were synthesized and simulated using Cadence<sup>®</sup> IC Design Framework and the 0.35µm AMS CMOS process parameters. This section, presents  $\omega_o$  and Q tunability, dynamic-range and Monte-Carlo results for a 4<sup>th</sup>-order (i.e. an 8<sup>th</sup>-order cascaded filter structure) OZGF. The filter was implemented using PMOS devices, due to their separate well connections (in the WI region, it is required that  $V_{BS} = 0$ to ensure accurate exponential/logarithmic conformity). The dimensions of the PMOS devices were set to 300µm/1.5µm in order to extend the WI region to the  $\mu$ A range and reach sub-millivolt matching. All NMOS devices (used in current mirrors not shown in Figs.8 and 9) have dimensions 60µm/8µm. Most transistors were in fact cascoded to reduce  $V_{DS}$  variations but we chose not to include them in the schematics for simplicity and clarity. The power supply and the capacitors were set to 1.8V and 20pF respectively.

#### A. Frequency Response

Figs.10 and 11 show  $\omega_o$  and Q tunability of the OZGF structure (transfer function 1.10). In Fig.10,  $I_o$  was varied from 2nA to 20nA, while  $I_Q$  was set to 2nA (so the Q gradually changes from 1 to 10). In Fig.11,  $I_o$  was fixed at 20nA, while  $I_Q$  was varied from 2nA to 20nA. Large-signal verification of the frequency response was also carried out.



Figure 10.  $\omega_o$  tunability by means of biasing current  $I_o$  of the 4<sup>th</sup>-order CMOS-WI log-domain Class-AB OZGF.



Figure 11. Q tunability by means of biasing current  $I_Q$  of the 4<sup>th</sup>-order CMOS-WI log-domain Class-AB OZGF.

#### B. Linearity, Noise and Power Consumption

The linearity of the whole structure was assessed by performing single-tone tests and reporting the value of the *THD* for various input strengths<sup>1</sup>. The tone's frequency was set at the peak of the passband. We report results for two such tests; one for the low-Q and one for the high-Q response. The minimum signal that the structure can process is determined by its input noise floor. The total input-referred noise floor was determined by integrating within the 3dB bandwidth. The noise floor value used to determine the input dynamic range corresponded to that of the high-Q situation, since in practice the structure will automatically adapt itself (through an AGC mechanism) to amplify small signals. Table 1 summarizes the performance of the reported 4<sup>th</sup>-order OZGF.

TABLE I.	OZGF	SIMULATED	PERFORMANCE
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Nominal Values	$f_{MAX} = 3.069 \text{ KHz}$ $I_o = 20 \text{ nA}; C = 20 \text{ pF}$ $Q = 1; V_{DD} = 1.8 \text{ V}$	$f_{MAX} = 4.15 \text{ KHz}$ $I_o = 20 \text{ nA}; C = 20 \text{ pF}$ $Q = 10; V_{DD} = 1.8 \text{ V}$
Power Consumption	3.67µW	3.728µW
Gain deviation	4.4%	1.13%
Input-Referred Noise	110pA	13.2pA
Linearity	THD @ m=350: 4%	THD @ m=0.01: 1%

As explained above, the input dynamic range of the system is defined by the following relation:

$$DR = \frac{m * I_{o} \text{ (for lowest } Q \text{ and } THD = 4\%)}{\text{noise floor (for highest } Q)}$$
(1.16)

From Table 1 and (1.16), the simulated input dynamic range of the 4<sup>th</sup>-order OZGF is found to be **114.5dB**.

## C. Monte-Carlo

This section presents indicative Monte-Carlo results to show how process and mismatch variations affect the filter's frequency response for the chosen device dimensions. Fig.12 shows the peak gain distribution of 200 simulation runs.



Figure 12. Monte-Carlo simulation results showing the peak gain distribution of the  $4^{th}$ -order CMOS-WI log-domain Class-AB OZGF with a Q of 10. Out of 200 runs, 156 filters had peak gains ranging from 72 to 82 dB. The theoretically calculated peak value is at 80dB.

#### V. CONCLUSIONS

We have presented the DAPGF and OZGF responses which closely resemble the behavior observed from the biological cochlea. Their form and simple parameterization seem to render them ideal candidates for efficient analog VLSI implementations. The adopted log-domain paradigm has proven to be an excellent design route towards the implementation of high-dynamic range frequency shaping networks, because of the companding nature of the resulting filter topologies. The designed Class-AB pseudo-differential log-domain OZGF has a simulated input dynamic range of 114.5dB, while dissipating on average only 3.7µW; these results compare well with the reported performance of the healthy mammalian cochleae. A novel AGC mechanism to automatically adjust the gain of the filter according to the input strength has already been designed. The whole closedloop system is currently being fabricated and will be incorporated in a filterbank architecture to realize superior performance bionic ear processors for applications such as speech recognition front-ends, portable health-care devices and implants for the hearing impaired.

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<sup>&</sup>lt;sup>1</sup> The input amplitude was set to  $m^*I_o$ . Thus, the index *m* indicates how many times larger or smaller is the input zero-to-peak amplitude relative to the biasing current  $I_o$ .